# A Novel Breast mass segmentation method based on patch merging and GHFCM

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#### Abstract

Breast cancer is regarded as one of the most frequent mortality causes among women. It is very important to create a system to diagnose suspicious masses in mammograms for early breast cancer detection. In this paper, we propose an automatic breast mass segmentation method based on patch merging method and generalized hierarchical Fuzzy C Means (GHFCM). The patch merging method is used to obtain the adaptive region of interest (ROI), while the GHFCM method which is able to overcome the drawbacks of effect of image noise and Euclidean distance FCM which is sensitive to outliers is used to obtain the precisely mass segmentation results. The new method is evaluated over MiniMIAS dataset. The segmentation performance from experimentations demonstrates that our method outperforms the other compared methods.

**Keywords:** Breast mass segmentation, Hierarchical distance function, Generalized mean, Patch merging, GHFCM

#### 1. Introduction

According to American cancer society, breast cancer is the most commonly diagnosed cancer type among women [1]. The early detection of breast cancer is the main way to increase recovery rate from disease. One of the ways to detect the breast cancer in early stages is to using mammography which is thought of as one of the most effective methods for breast cancer diagnose [2]. Recent developments in digital mammography imaging systems have aimed to better diagnosis of abnormalities in the breast and have increased the survival chance [3]. Nowadays, computer-aided diagnosis (CAD) system is widely used to assist the radiologists in breast masses detection and identification. CAD system which seem appealing to the radiologists generally consists of segmentation, feature extraction and classification stages [4]. Precisely breast masses segmentation in mammograms plays a critical role in the whole system and successfully influences the consequent stages.

In the past, many automatic or semi-automatic breast mass segmentation methods have been widely proposed. In these methods, one type of two step segmentation strategy is a very common mass segmentation pattern. These two steps contain the ROI generation which is cropped from the breast area and the mass boundary detection in ROI. Region growing method which using a similarity measure of the two adjacent pixels to group the pixels is used to generate the ROI in breast area [5-6]. However, this method is very sensitive to the noise and local optimum. In this paper, patch based method is used for ROI generation at first to overcome the effect of the noise.

After ROI generated, some boundary detection methods based on pattern recognition algorithms [7-11] can be used to segment the breast mass from ROI. In [12], a semi-automatic region growing approach is proposed based on the choice of the starting point by the radiologist. In [13], Kobatake, *et al.*, applied a modified Hough transform to

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extract lines passing near the centre of the mass and automatically selected candidates based on the number of line-skeletons. In [15], Elter, *et al.*, proposed a contour tracing approach to extract shape of the region. The ROI of mass is transformed into polar coordinate system, and then contour of estimated mass is calculated by using a shortest path algorithm. In [15], Tao, *et al.*, proposed a classification system to identify spiculation of a mass by integrating machine learning method and graph-cut algorithm. Tolga, *et al.*, [16] proposed a breast mass contour segmentation method based on classical seed region growing with additional capability of adaptive threshold value to extract optimum contour information. Song, *et al.*, [17] use a plane fitting method based on dynamic programming optimization approach to propose a breast mass segmentation method.

As a classification method, FCM algorithm which have been widely studied and successfully applied in image clustering and segmentation is also able to detect the breast mass. However, the traditional FCM algorithm is very difficult to obtain the accurate mass segmentation results due to overlapping intensities, low contrast of images, and especially the noise perturbation. To overcome the effect of the noise, a wide variety of approaches have been proposed to incorporate spatial information in the image [18-19]. In [20], Zheng, *et al.*, proposed two algorithms, generalized FCM (GFCM) and hierarchical FCM (HFCM), then integrated them to propose GHFCM method to overcome the effect of noise and outliers. In this paper, we propose an automatic breast mass segmentation method based on patch merging method and generalized hierarchical FCM (GHFCM). The patch merging method is used to obtain the adaptive ROI, while the GHFCM method is used to obtain the precisely mass segmentation results. The new method is evaluated over MiniMIAS dataset. The segmentation performance from experimentations demonstrates that our method outperforms the other compared methods.

The advantages of our method are can be explained in three aspects. First, using patch merging method as the initial step to provide ROI can improve efficiency since the number of operated units is observably reduced. Second, GHFCM clustering process in ROI for detecting breast mass is much faster than that in the whole image since we avoid the abundant calculation of pixels which is outside the ROI. Finally, by combining the general FCM (GFCM) which is robust to the noise with the spatial constraints and hierarchical FCM (HFCM) which is robust to the outliers with the a general and flexible distance function to introduce a generalized hierarchical FCM (GHFCM), the breast mass segmentation results can be more accurately obtained in ROI generated in the first step.

#### 2. Our Method

#### 2.1 ROI Generation using ISODATA Clustering and Patch Merging

In mammograms, there are two different parts: one is breast tissue region which containing the breast mass and another one is non-breast tissue region which takes up a large region in the image. To effectively segment the breast mass, we need to firstly preprocess the mammogram and select a ROI which only contain the whole breast mass and breast normal tissue. In this subsection, we introduce a patch merging method to generate ROI.

Patches taken inside images, are at the very heart of many image processing applications [21], such as texture synthesis [22], image inpainting [23], image restoration [24]. The advantage of using patches to process the image is that it takes of very important image feature and is robust to the noise. Let N(x) be image patch of the pixel x, the image can be divided into lots of similar patches with same size. Then we transform the patch N(x) to a vector form V(x) and use ISODATA algorithm [25-26] to classify the vectors from all the image patches. ISODATA method is a method which added division

of a cluster, and processing of fusion to the K-means method. The procedure of the ISODATA method is shown as follows:

#### **Algorithm 1: ISODATA clustering**

- 1. Choose randomly  $K = K_0$  initial mean vectors  $\{m_1, m_2, \dots, m_k\}$  from the dataset.
- 2. Assign each patch V(x) of data point x to the cluster with closest mean:

$$x \in \omega_i \text{ if } d(V(x), m_i) = \min\{d(V(x), m_1), \dots, d(V(x), m_k)\}\$$

- 3. Discard clusters containing too few members, i. e., if  $n_j < n_{\min}$ , then discard  $\omega_j$  and reassign its members to other clusters.  $K \leftarrow K-1$ .
- 4. For each cluster  $\omega_i(j=1,\dots,K)$ , update the mean vector

$$m_j = \frac{1}{n_j} \sum_{x \in \omega_j} V(x)$$

and the covariance matrix:

$$\Sigma_{j} = \frac{1}{n_{j}} \sum_{x \in \omega_{j}} (V(x) - m_{j}) (V(x) - m_{j})^{T}$$

The diagonal elements are the variance  $\sigma_1^2, \dots, \sigma_N^2$  along the *N* dimensions.

5. If  $K \le K_0/2$  (too few clusters), go to Step 6 for splitting;

else if  $K \ge 2K_0$  (too many clusters), go to Step 7 for merging;

6. For each cluster  $\omega_j$   $(j=1,\dots,K)$ , find the greatest covariance  $\sigma_m^2 = \max\{\sigma_1^2,\dots,\sigma_N^2\}$ 

If  $\sigma_m^2 > \sigma_{\text{max}}^2$  and  $n_j > 2n_{\text{min}}$ , then split into two new cluster centers

$$m_i^+ = m_i + \sigma_m$$
,  $m_i^- = m_i - \sigma_m$ 

Alternatively, carry out PCA to find the variance corresponding to the greatest eigenvalue  $\lambda_{max}$  and split the cluster along the direction along the corresponding eigenvector.

Set  $K \leftarrow K+1$ 

Go to Step 8.

7. (merge) Compute the K(K-1)/2 pairwise Bhattacharyya distance between every two cluster mean vectors:

$$d_{B}(\omega_{i},\omega_{j}) = \frac{1}{4}(m_{i} - m_{j})^{T} \left[\frac{\Sigma_{i} + \Sigma_{j}}{2}\right]^{-1} (m_{i} - m_{j}) + \log \left[\left|\frac{\Sigma_{i} + \Sigma_{j}}{2}\right|\right/ (|\Sigma_{i}, \Sigma_{j}|)^{1/2}\right], \ 1 \leq i, j \leq K, \ i > j$$

For each of distances satisfying  $d_B(\omega_i,\omega_j) < d_{\min}$ , merge of the corresponding clusters to form a new one:

$$m_i = \frac{1}{n_i + n_j} [n_i m_i + n_j m_j]$$

Delete  $m_i$ , set  $K \leftarrow K-1$ 

8. Terminate if maximum number of iterations is reached. Otherwise go to Step 2.

After the ISODATA clustering finished in the mammograms, we use the patch which contains the seed point and its neighborhood patches to construct a ROI to improve the segmentation efficiency. The patch is considered to be the neighborhood of the patch which contains the seed point if the distance between its center and the seed point is small than an acceptable limits and its label is same as seed point label. After that, a rectangle which exactly surround all above patches is selected as ROI for following breast mass segmentation. Figure 1 demonstrates the ROI generation results of different mammograms. The advantage of our ROI selected method is that the ROI is adaptive to the breast mass.

### 2.2 Breast Mass Segmentation in ROI using GHFCM

After ROI generation, we can segment the breast mass in ROI instead of the whole image domain to improve the efficiency. The clustering algorithms such as FCM or GMM can be use to perform this task. However, without the spatial prior knowledge, these clustering algorithms are still weak in imaging noise, outliers and other imaging artifacts. To overcome these drawbacks, a GHFCM which is proposed in[20] is applied to segment the breast mass in ROI. In [20], the generalized mean is incorporated into FCM to propose GFCM at first. Then, the distance function is estimated by a sub-FCM to propose HFCM. At last, GFCM and HFCM are combined to introduce Generalized Hierarchical FCM (GHFCM) to overcome the effect of image noise and outliers.

#### 2.2.1 **GFCM**

In GFCM, the distance function of FCM is improved by using local generalized mean and the new object function is presented as follows:

$$J_{m}^{GFCM} = \sum_{i=1}^{N} \sum_{j=1}^{J} u_{ij}^{m} \sum_{c \in N_{i}} w_{c} d_{cj}$$
 (1)

where  $w_c$  is the weighted factor to control the influence of the neighborhood pixels depending on their distance from the central pixel i. The strength of  $w_c$  should decrease as the distance between pixel c and i increase. In [20], Gaussian function is used to construct  $w_c$ :

$$w_c = 1/(2\pi\delta^2)^{1/2} \exp(-d_{ci}^2/2\delta^2)$$
 (2)

By applying local weighted generalized mean on membership, the modified membership  $u_{ij}$  can be calculated as:

$$u_{ij} = \sum_{c \in N_i} w_c u_{cj} / \sum_{h=1}^{J} \sum_{c \in N_i} w_c u_{ch}$$
 (3)

From Eq. (3), the new membership incorporating image spatial information according to the help of local weighted generalized mean, makes the algorithm is more robust to image noise.

#### **2.2.2 HFCM**

To overcome the outliers, the distance function in traditional FCM is assumed to be a sub-fuzzy model and generate the HFCM. The object function of HFCM is given as:

$$J_{m,n}^{HFCM} = \sum_{i=1}^{N} \sum_{i=1}^{J} \sum_{k=1}^{K} u_{ij}^{m} v_{ijk}^{n} \overline{d}_{ijk}$$
 (4)

It can be seen that at the second level of the hierarchy, information is provided about the data along with their class labels. It is noted that we have J classes; K subclasses correspond to each class of the first level. Using Euclidean distance  $\overline{d}_{ijk} = \|y_i - \mu_{jk}\|^2$ , and the presentation form of  $\mu_{jk}$  is given as

$$\mu_{jk} = \sum_{i=1}^{N} u_{ij}^{m} v_{ijk}^{n} y_{i} / \sum_{i=1}^{N} u_{ij}^{m} v_{ijk}^{n}$$
 (5)

By assuming each cluster to contain several sub-clusters, HFCM is robust to the outliers.

#### **2.2.3 GHFCM**

The generalized hierarchical FCM (GHFCM) is generated by combining HFCM and GFCM, and its objective function can be given as

$$J_{m}^{GHFCM} = \sum_{i=1}^{N} \sum_{j=1}^{J} \sum_{k=1}^{K} u_{ij}^{m} v_{ijk}^{n} \sum_{c \in N_{i}} w_{c} d_{cjk}$$

$$= \sum_{i=1}^{N} \sum_{j=1}^{J} \sum_{k=1}^{K} \sum_{c \in N_{i}} u_{ij}^{m} v_{ijk}^{n} w_{c} \left\| y_{c} - \mu_{jk} \right\|^{2}$$
(6)

The membership  $u_{ij}$  and sub-membership  $v_{ijk}$  satisfies the constraint  $\sum_{j=1}^J u_{ij} = 1$  and  $\sum_{k=1}^K v_{ijk} = 1$ , respectively. By applying the optimization way similar to the standard FCM, the parameters in GHFCM can be calculated iteratively as

$$u_{ij} = \left(\sum_{k=1}^{K} \sum_{c \in N_i} w_c v_{ijk}^n d_{cjk}\right)^{1/(1-m)} / \sum_{h=1}^{J} \left(\sum_{k=1}^{K} \sum_{c \in N_i} w_c v_{ijk}^n d_{cjk}\right)^{1/(1-m)}$$
(7)

$$v_{ijk} = \left(\sum_{c \in N_i} w_c u_{ij}^m d_{cjk}\right)^{1/(1-n)} / \sum_{k=1}^K \left(\sum_{c \in N_i} w_c u_{ij}^m d_{cjk}\right)^{1/(1-n)}$$
(8)

The cluster center  $\mu_{ik}$  is evaluated as

$$\mu_{jk} = \sum_{i=1}^{N} \sum_{c \in N} u_{ij}^{m} v_{ijk}^{n} y_{c} / \sum_{i=1}^{N} u_{ij}^{m} v_{ijk}^{n}$$
(9)

According to [20], using local weighted generalized mean to incorporate spatial information and cluster information, the modified membership and sub-membership can be re-calculated as:

$$u_{ij} = \sum_{c \in N_i} w_c u_{cj} / \sum_{h=1}^{J} \sum_{c \in N_i} w_c u_{ch}$$
 (10)

$$v_{ijk} = \sum_{c \in N_i} w_c v_{cjk} / \sum_{h=1}^K \sum_{c \in N_i} w_c v_{cjh}$$
 (11)

For breast mass segmentation in ROI, we set J = 2 to represent breast tissue and breast mass in ROI and K = 2 to be the number of each sub-cluster. The integrated GHFCM algorithm is given as:

## **Algorithm 2: GHFCM Algorithm**

- 1. Fix the cluster number J=2, the sub-cluster number K=2, initialize fuzzy membership, sub-membership and then select initial cluster center.
  - 2. Set the loop counter l = 0.
  - 3. Update the new cluster center using Eq. (9)
  - 4. Update the fuzzy membership function using Eq. (7) and Eq. (10).
  - 5. Update the fuzzy membership function using Eq. (8) and Eq. (11).
- 6. Terminate the iterations if the object function converges; otherwise, increase the iteration (l = l + 1) and repeat Steps 3 through 6.

## 3. Implementation and Experiment Results

In this section, we experimentally evaluate our proposed GHFCM in a set of synthetic images and real images. The neighborhood window size of GHFCM is set as  $5\times5$ .

Figure 1 demonstrates the outputs at first step of our method for three real mammograms. The first column shows the original mammogram with breast mass. The second column shows the corresponding ROI generated by ISODATA clustering and patch merging. The advantage of our ROI selected method is that the ROI is adaptive to the breast mass. The ROI which is used to replace the whole image domain for breast mass segmentation can improve the segmentation efficiency.

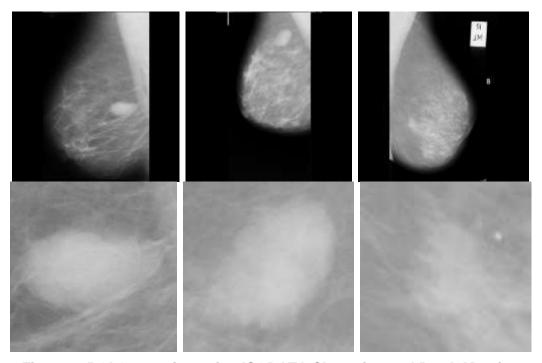
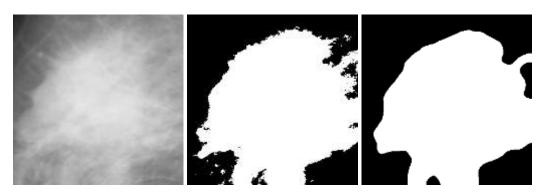


Figure 1. ROI Generation using ISODATA Clustering and Patch Merging

Figure 2 demonstrates the segmentation results of our method and the comparison with Gaussian mixture model (GMM). The first column demonstrates the ROIs of four mammograms from MiniMIAS dataset with different mass shapes. The second column shows the segmentation results obtained by GMM. From these results, we can see that the GMM model which is sensitive to the noise and outliers, cannot obtain a smooth boundary of breast mass. The third columns show the segmentation results of our method. These segmentation results indicate that our method which integrates the spatial constrain and hierarchical clustering strategy is robust to noise and outliers and is able to obtain a very smooth boundary of breast mass. For quantitative analysis, we calculate the Dice score of each method on eight original mammograms, the related results are shown in Figure 3. We can see that the Dice value of each segmentation result obtained by our method is much higher than that of result obtained by GMM, which indicates the superior performance of our segmentation method for breast mass segmentation.



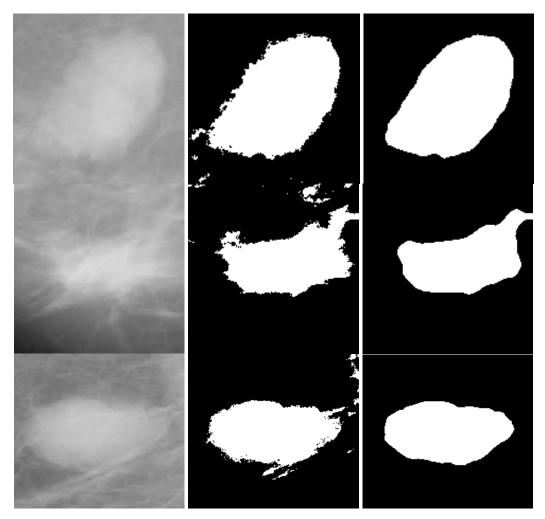


Figure 2. Comparison Results of Breast Mass Segmentation

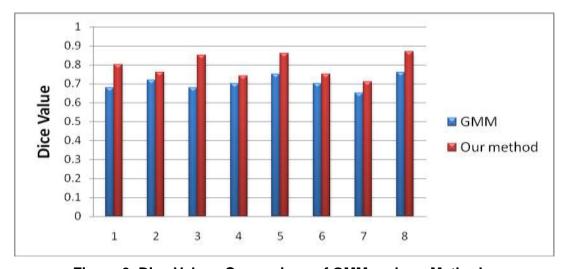


Figure 3. Dice Values Comparison of GMM and our Method

## 4. Conclusions

In this paper, we propose an automatic breast mass segmentation method based on patch merging method and GHFCM. The ISODATA clustering and patch merging

method is used to obtain the adaptive ROI and initial segmentation results, while the GHFCM method which is able to overcome the drawbacks of effect of image noise and Euclidean distance FCM which is sensitive to outliers is used to obtain the precisely mass segmentation results. The new method is evaluated over MiniMIAS dataset. The segmentation performance from experimentations demonstrates that our method outperforms the other compared methods.

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